# Computational Modeling of the Cardiovascular System

# Modeling of Force Development in Myocytes



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# Hill's Model of Muscle Contraction (1924/1938)

#### Measurement

- Muscle is fixed at length  $I_0$
- Electrical stimulation



CVRT

Isometric, Tetanus with max. mechanical tension  $P_o$ 

- Release of fixation
  Force *F* is applied with *F=mg* g: Gravitational constant
  m: Mass
- Measurement of time t, when muscle passes mark at length I
- Calculation of velocity

$$v = \frac{l_0 - l}{t}$$



## **Relationship between Mass and Contraction Velocity**



# **Modeling of Muscle Contraction**



# Model Extension: Hill's 3-Element Model (1970)

#### Limitations of Hill's Model

- only force-velocity relationship
- only tetanized muscle, no information of partial or relaxed muscle
- only serial elastic element
- only quick responses

#### Hills 3-Element Model

inclusion of parallel elastic element

# Further extensions necessary for realistic modeling of cardiac muscles!





## Sarcomeres in Cardiac Muscle (Fawcett & McNutt 1969)



# Sarcomeres in Skeletal Muscle (Fawcett & McNutt 1969)



# Sarcotubular System T system (transverse tubule) Sarcoplasmic reticulum (longitudinal tubule) Sarcolemma (cell membrane) Triad (skeletal muscle) Dyad (cardiac muscle) Mitochondrion (modified from Porter and Franzini- Armstrong)







#### **Proteins of Sarcomere**



#### **Involved Proteins and Regulation of Force**





# **Contraction of Myocyte by Electrical Stimulation**



Microscopic imaging of isolated ventricular cell from guinea pig http://www-ang.kfunigraz.ac.at/~schaffer



## Measurement of Force Development in Single Cell



# **Measurement Techniques**

Permeabilization of sarcolemma/skinning of myocytes by saponin or Triton X-100

Direct control of intracellular concentrations of ions, drugs etc.

 $\left[Ca^{2+}\right]_{i} = \left[Ca^{2+}\right]_{o}$ 

Transillumination of myocyte or muscle strands with laser light

Diffraction pattern ~ sarcomere length





#### Sarcomere Length Measurement via Laser Diffraction



FIGURE 2. Diffraction spectra obtained from a thin, right-ventricular rat trabecula. The two first-order diffracted lines  $(\pm 1)$  were symmetrically spaced on either side of the central bright line of nondiffracted light (zero order). The distance between the zero-order line and the first-order lines are inversely related to sarcomere length.

(Figures from Lecarpentier et al., Real-Time Kinetics of Sarcomere Relaxation by Laser Diffraction, AJP, 1985)

More information: http://muscle.ucsd.edu/musintro/diffraction.shtml





**EXEMPT 1.** Experimental set-up. Abbreviations are: I, laser; MI, microscope; V, video camera; MC, muscle chamber; B, beam splitter; W, densitometric wedge; F, split;  $D_1$  and  $D_2$  diodes; g and h, optical signals electronically converted by  $D_1$  and  $D_2$  respectively; g/h, signal function of sarcomere length; T, electromagnetic transducer;  $B_2$  stimulator; M, muscle tension and shortening curves vs. time (0); S, instantaneous sarcomere length curve vs. time (0).

# **Force Development: Sliding Filament Theory**

Cellular force development by sliding myofilaments (Huxley 1957), i.e. actin and myosin, located in sarcomere



Attachment of myosin heads to actin



Filament sliding





## **Force Development: Sliding Filament Theory**



# **Actin-Myosin Interaction**



## **Coupling of Electrophysiology and Force Development**





# **Calcium Handling and EC-Coupling**



# **Group Work**

Which states are important for a detailed modeling of force in myocytes?

Which states can be neglected for an efficient model?



# **Models of Force Development**



CVRT

# Mathematical Modeling of Myofilament Sliding (Huxley)



## **Modeling of Cellular Force Development**



#### 4-State Model of Force Development: State Diagram



#### Description by set of 1st order ODEs

- Transfer of states N0, N1, T0, and T1 is dependent of rate coefficients
- Rate coefficients are partly function of intracellular calcium [Ca<sup>2+</sup>]<sub>i</sub>

(Model 1 of Rice 1999 et al./ Landesberg et al.1994)



# **4-State Model of Force Development**

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Several states contribute to force development:

Force is dependent on overlap of actin and myosin filaments.

Frank-Starling Mechanism

Force ~ initial length

Diastolic volume ~ cardiac output



Sarcomere length  $[\mu\,m]$ 



#### **4-State Model of Force Development: Matrix Notation**



Numerical solution e.g. with Euler- and Runge-Kutta-methods



#### State Diagram of 3rd Model of Rice 1999 et al.



# Matrix representation of State Diagram



#### Force Development for Different Static Sarcomere Lengths (SL)



#### Model of Glänzel et al. 2002: Activation



#### Model of Glänzel et al. 2002: Crossbridge Cycling



## **Reconstruction of Static Measurements**



# **Reconstruction of Length Switch Experiments**

#### Study

- · Species: rabbit
- Ventricular myocytes

# Length Switch Experiment

- Stretch of 4.6% in 10 ms
- Return to original configuration in 10 ms





#### Coupling of Force with Electrophysiological Models: Basics



## Coupling of Force with Electrophysiological Models



## Coupling of Force with Electrophysiological Models



## Coupling of Force with Electrophysiological Model: Human



## Modeling Force Development with Cellular Automaton

#### Anatomical Model



# Physiological Parameters

#### Cellular Automaton



- Transmembrane voltage
- Calcium concentration





CVRTI



# **Modeling of Force Development: Sinus Rhythm**







## **Modeling of Force Development: Coupling**



# **Group Work**

Discuss the application of cellular automata for simulation of electrophysiology and force development.

Which simulations are more realistic?

